SUMMARY OF SCIENTIFICAL RESULTS

BioHPP Study Results 2011-2018

BioHPP – The New Material Class in Prosthetics
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Bibliography
Foreword

Physiological scaffold materials adapted to nature – from PEEK to BioHPP

For over 35 years, PEEK has been used as an implant material in human medicine (finger prostheses, intermediate spinal bodies, and hip joint prostheses). The advantages lie in the highly bio-compatible material properties that allow the prostheses to be integrated into the bone. The mechanical material properties are also highly similar to those of the bone skeleton.

PEEK (polyetheretherketone) is a high-performance polymer from the group of polyaryletherketones and is their most important representative. PEEK is a bioinert material that can be used for implantation in the human body. Its elasticity is more similar to that of human bone than titanium-based alloys, such as those used to replace joints, for example.

If PEEK is used as implant abutment instead of such alloys, this reduces the stress on the bone and the tissue compared with metallic materials. As a result, the risk of bone resorption by implants is reduced. Whereas PEEK has been used in surgery for the indications mentioned above for decades, the material has not been used in dentistry for that long. For the prosthetic supply of medical devices based on PEEK, bredent distributes the material BioHPP in the form of pellets, granules, and milling blanks for processing in the dental laboratory.

BioHPP is a specially modified PEEK enriched with inorganic fillers (approx. up to 30%) and approved for dental applications (Medical Devices Act Class IIb). Bredent thus modified the material-specific properties for use as a scaffold material. The biological properties of the base polymer PEEK were not changed but rather significantly improved in terms of material combinations (e.g. veneering composites and adhesive composite systems) and mechanical properties (e.g. elasticity and bending strength). This summary of various scientific studies shows the properties and the advantages compared to the usual materials such as zirconia dioxide and dental casting alloys.

Your bredent group
Classification of industrial polymers

The term “high-performance polymers” is often misunderstood in the dental industry. From a chemical point of view, the term is derived from the continuous service temperature, which is above 150°C. In combination with the excellent mechanical properties PEEK is in a class of its own compared with standard and technical polymers. Thanks to the admixture of inorganic fillers, BioHPP is also in the highest class and far exceeds the material-specific properties of PEEK. With its mechanical advantages (e.g. excellent polishability and composite materials), BioHPP is particularly suitable for use in the dental sector.

![Polymer pyramid](image)

Fig. 1: The polymer pyramid illustrates the classification of standard polymers, technical polymers, and high-performance polymers.
SUMMARY OF SCIENTIFIC RESULTS

1 Determination of material properties of BioHPP\textsuperscript{1,2)\textsuperscript{1}}

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Polyclinic for Dental Prosthetics and Materials Science

The aim of the work was the investigation of the PEEK plastic BioHPP in the colour white. In addition to bending strength, modulus of elasticity, and hardness, its surface, abrasion, and discolouration properties as well as the bond strengths to form cement composites were investigated.

Abrasion resistance of BioHPP compared with various veneering composites and amalgam as a filling material

The abrasion resistance was determined using the 3-media abrasion machine (Willytec) according to the abrasion method developed by De Gee. The specimen wheel was equipped with test specimens; an AlMg alloy of the same hardness as amalgam and Gradia dentin mass was used as a reference material. After grinding in the equipped wheel with a coarse and then fine diamond grinding wheel (contact pressure = 15 N), an abrasion test with a contact pressure of 20 N was carried out. The intermediate medium was dentifrice body HS RMS 1100015. The abrasion tendency of BioHPP (Fig. 2) was comparatively low at 1.5 (AlMg alloy of the same hardness as amalgam = 1). From this, it can be deduced that occlusal surfaces made of BioHPP are less abrasively damaged than with other veneering resins. Conversely, the vital teeth in contact with BioHPP are also less worn than is the case with ceramic materials, for example.

![Fig. 2: Principle of the 3-media abrasion machine developed according to De Gee (Willytec).](image)

![Grade of abrasion](image)

![Fig. 3: Abrasion tendency of BioHPP and various veneering composites compared with AlMg alloy.](image)

\textsuperscript{3} Rzanny, Werkstoffkundliche Untersuchungen, 2013, 5.
\textsuperscript{4} Rzanny, PEEK – ein interessanter Werkstoff, ZWR 2015, 611.
\textsuperscript{5} Rzanny, Werkstoffkundliche Untersuchungen, 2013, 9.
\textsuperscript{6} Ebd., 12.
To determine the exogenous tendency to discolouration, the test specimens were stored for 4 weeks at 37°C in various preparations (coffee, tea, tobacco, red wine, methylene blue, and distilled water). The measurement of discolouration in comparison to the control (stored dry and dark at 37°C) was performed with the ShadeEye-NCC (Shofu, Ratingen). This works on the basis of the CIELAB system and determines the L*a*b* values, which provide information on hue, brightness, and saturation. The scatter of the L*a*b* values around the control sample was calculated on the basis of the standard deviation. The resulting value is called degree of discolouration $V$. In order to record the total deviation of the discoloured specimen from the control specimen, the colour difference $\Delta E$ was calculated from the 3 components. $\Delta E$ is a measure of the visually discernible colour difference under the most favourable conditions.

The average exogenous discolouration tendency of the media examined (coffee, tea, tobacco, red wine, and methylene blue) was very low for novo.lign and BioHPP (1.2 and 2.8, respectively; Fig. 4).

A very smooth surface is the most important prerequisite for a low plaque build-up. This is the only way to keep the denture clean for a long time and make cleaning easier. Test specimens of 20 mm length, 10 mm width and 3 mm thickness were used to determine the surface quality, and the surface was treated as follows: A distinction was made between a dental technique without circular movement (A1), another dental technique with circular movement (A2) and a dental processing method (B).

The surface quality achieved surface roughness of 0.04 µm (Fig. 5) using both dental-technical and dental variants. In order to achieve this high surface quality, the polishing strategy had to be adhered to very precisely. With conventional polishing strategies for composites it is impossible to achieve an acceptable surface roughness.
Measurement of the composite strengths of BioHPP sample plates to various dental materials

The pressure shear tests were carried out with the Zwick Z 005 universal testing machine. The traverse speed was 1 mm/min. One to three test specimens (initial value) or four test specimens (artificial ageing) were produced per series. The adhesive strength of BioHPP was thus determined for the veneering composite combo.lign and the cement composite DTK adhesive. The test specimens made of BioHPP were produced using different processes. In the first process, mechanical macro retentions in the form of beads and crystals were applied using the pressing technique. In the versions milled using CAD/CAM, the specimen surfaces were smooth.

The platelet surface of all samples was blasted with corundum (110 μm; 3 bar) see also fig. 7 and 9a:

1. BioHPP (milled): 20 × 10 × 2 mm, visio.link (90 s Dentacolor XS), combo.lign was applied. This was stored for 10 min in the dark and then exposed to Dentacolor XS for 90 s.

2. BioHPP (pressed with beads): 20 × 10 × 2 mm, visio.link (90 s Dentacolor XS), combo.lign opaque (90s Dentacolor XS), combo.lign was applied to a metal ring placed on the BioHPP surface. This was stored for 10 min in the dark and then exposed to Dentacolor XS for 90 s.

3. BioHPP (pressed with crystals): 20 × 10 × 2 mm, visio. link (90 s Dentacolor XS), combo.lign opaque (90 obligations Dentacolor XS), combo.lign was applied to a metal ring placed on the BioHPP surface. This was stored for 10 min in the dark and then exposed to Dentacolor XS for 90 s.

The bond strength of BioHPP to the cementing composite combo.lign is shown in Fig. 9a. The pressure-shear strength of 25 MPa remained stable even after artificial ageing. The macro retentions applied (beads, crystals, see Fig. 7) led to a significant increase in the network to up to 40 MPa. The adhesive strengths of BioHPP on titanium and zirconia dioxide surfaces determined in vitro (adhesive: DTK adhesive) is shown in Fig. 8. For titanium and zirconia dioxide, 25 and 32 MPa, respectively were measured; this did not show any significant decrease in adhesion, even after 25,000 TLW.
Common framework materials such as precious metal, zirconia dioxide or NPM show similar or lower bond strength values (Fig. 9b). The composite strength of the materials to the veneering material combo.lign was also tested after artificial ageing and 25,000 temperature load changes. A clinically safe level of bond strength according to DIN EN ISO 10477:2005-01 is achieved at 20 to 22 MPa.

Editor’s note: “A good bond to both the veneering material and the fixing material is decisive for the wearing time and durability of the denture. Increasing the surface roughness is a necessary prerequisite for good adhesion.”

Fig. 9b: Combo.lign compression shear strength to metallic framework materials and polymers.11)
2 In-vitro-investigations of BioHPP in telescope technology\textsuperscript{12)}

The aim of the present work was to measure the pull-off force of cylindrical single telescopes. The influence of ageing and the hydraulic effect on adhesion were tested. In this study it was examined which material combinations lead to material abrasion or friction loss taking into account the integration frequency. An optimal material pairing of primary and secondary telescope was derived from these results. The initial pull-off forces were between 2 and 3 Newton. In a single-tooth telescope, a higher value can lead to damage to the periodontium. In addition, the ideal manufacturing specifications for BioHPP secondary components with regard to the adjustment of embedding material, preheating temperature, and finishing of the inner surfaces were tested and determined.

Analysis of friction curves taking into account different dental scaffold materials

The holding force of cylindrical telescopic crowns (diameter = 6 mm, height = 5 mm) was measured dry and under water in the tensile test. To check the influence of ageing, the crowns were joined and separated repeatedly (nmax=10,000 cycles). In the course of the first 100 joining cycles, the adhesive force was measured for the first time after 10 pulls. The holding force was then measured once after 1,000 and 10,000 cycles. For some crowns, the pull-off speed was varied during the first tests (10 to 200 mm/min) in order to check the hydraulic influence on the adhesion of the telescopic crowns.

\[\text{Fig. 10: Primary components made of three different scaffold materials.}^{13}\]\n
\textsuperscript{13) Faber, In-vitro-Untersuchungen in der Teleskoptechnik, 2013.} 
\textsuperscript{14) Ebd.} 
\textsuperscript{15) Ebd.}
After 10,000 wear cycles, all telescope systems showed clinically acceptable pull-off forces on average. The adhesive forces of all test specimens increased during the first 1,000 cycles. After this, the adhesive forces of the secondary components on BioHPP primary components remained more or less constant. The adhesive forces of the secondary components on NPM and zirconia oxide primary components showed a higher variability ranging from 0.72 to 13.15 N. With regard to the adhesive forces measured, the material BioHPP can be used as a definitive telescopic crown material. In combination with primary components made of harder materials such as zirconia dioxide or NPM, a higher scattering of the pull-off forces can be expected. The use of BioHPP primary components with BioHPP secondary components is to be preferred.

Editor’s note: “The results show that primary and secondary components made of BioHPP are the best combination in terms of loss of friction. This results in a very simple integration of the denture with optimum adhesion for the patient. The initial friction forces are adjusted by the expansion control during the manufacture of the secondary telescopes. Through the high gloss polishing of the inner surfaces with paint brushes, the total friction can be individually adjusted depending on the number of telescopes. Another advantage of BioHPP telescopes is the simplicity of manufacture. For example, it is possible to produce an alginate impression for fixed primary telescopes at a later date.”

Fig. 12: Pull-off forces (loss of friction) of telescopic crowns made of BioHPP on various primary crown materials (zirconia dioxide, CoCr, BioHPP (pressed), BioHPP (milled)).

Adhesion strength in [N]
3 Bond strength between PEEK and veneering resins depending on the surface preparation in the shear test according to EN ISO 10477\textsuperscript{16}

The test of the bond strength between a scaffold material (in this study, three different high-performance polymers) was determined by means of the pressure shear test, taking into consideration EN ISO 10477. The test specimens were made of three different PEEK scaffold materials (PEEK-Optima, BioHPP (milled), and BioHPP (pressed)). All 3 materials were conditioned differently (Al\textsubscript{2}O\textsubscript{3} and Rocatec) and then wetted and polymerised with three different bonding agents. Three different opaques (combo. lign, combo.lign Opaquer, and Sinfony) were then applied to these prepared surfaces. After the measurement, all samples were thermocycled (71 h at 37°C) in order to be able to draw conclusions about a wearing time of 5 years.

High-performance polymers based on PEEK are all opaque and are veneered with veneering composites for aesthetic reasons. The surfaces to be veneered are pretreated differently to increase the bond strength. In this paper, the bond strength of the scaffold material with commercially available veneering materials from various suppliers is evaluated depending on the conditioning.

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<table>
<thead>
<tr>
<th>Production Method</th>
<th>Surface Treatment</th>
<th>Supplier</th>
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<tr>
<td>milled</td>
<td>3) Rotatec\textsuperscript{16} Pre (110 µ) + Rotatec\textsuperscript{17} Soft (30 µ) + Al\textsubscript{2}O\textsubscript{3} (110 µ)</td>
<td>Invibio, Lancashire, United Kingdom</td>
</tr>
<tr>
<td>pressed</td>
<td></td>
<td>b) bredent medical, Senden, Germany</td>
</tr>
</tbody>
</table>

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\textsuperscript{17} Elsbernd (Schulte) F, Faber FJ, Roggendorf H. Bond Strength of different Composites to Polyetheretherketon (PEEK) (Poster). Köln: Universität zu Köln; 2015.
Analysis of the bond strength

Taking into account EN ISO 10477, all values are within ranges acceptable for clinical application. The only exception is the material combination combo.lign on BioHPP when using the bonding agent Solobond Plus. Comparable bond strengths to the metal–ceramic systems were only achieved using the bonding agent visio.link.

Editor’s note: “The results show that the conditioning of the BioHPP veneering surfaces in combination with a suitable primer and opaquer is extremely important. Because BioHPP is highly opaque when not veneered, it should be veneered in visible areas. Several veneering composites with special bonding agents are available. However, the highest bond strengths are achieved with the combination of visio.link bonding agent with combo.lign opaque. The modulus of elasticity of combo.lign has been adapted to that of BioHPP. This is the only way to avoid tensions and flaking veneers. The use of mechanical retentions additionally ensures the bond strength”.

Fig. 14: Depending on the composite system, the bond strength has significantly decreased after ageing because of thermocycling (n = 100). The best results were measured using visio.link (p < 0.05).

Fig. 15: The lowest bond strength values were measured when Solobond Plus was used after ageing. The results of combo.lign and Sinfony plus opaque are comparable.

Fig. 16: In combination with the bonding agent visio.link, bond strength values < 20 MPa are achieved. Only with the combination of PEEK Optima and Sinfony veneering composite do the values sometimes fall below 20 MPa after ageing.
4 Influence of production on the breaking load of three-unit PEEK bridges\textsuperscript{21)}

PEEK-based materials are increasingly being used in dentistry. The PEEK material BioHPP, which is reinforced with inorganic substances, can be processed in various ways: BioHPP can be pressed from granules or pellets or milled out of industrially manufactured CAD/CAM blanks. The aim of this study was to compare the stability of bridges made with these three manufacturing methods.

For the examination, 15 congruent bridges were fabricated three times. A standardized bridge model of region 24-26 was the basis (Fig. 17). After scanning (Ceramill Map 400, Amann Girrbach, Koblach, Austria), the bridges were constructed (Ceramill Mind, Design Software, Amann Girrbach) with a connector cross-section area of 16 mm\textsuperscript{2}. The occluso-gingival height of the connectors was 4.45 mm; the vestibulo-oral width was 3.60 mm. A slight indentation was constructed on the occlusal surface of the pontic so that a steel ball with a diameter of 5 mm was perfectly positioned at this point to determine the breaking load (Fig. 19).

This ensured a 3-point contact between the steel ball and the occlusal surface. With this data set, 15 bridges from the BioHPP blank (breCAM.BioHPP, bredent) and 30 bridges made of wax (breCAM.wax, bredent) were form ground on the milling machine (ZENO 4030 M1, Wieland Dental + Technik, Pforzheim).

According to the manufacturer specifications, supply channels to the object were waxed onto the wax bridges. The wax bridges were randomly divided into two groups and embedded with special muffles for BioHPP granules (bredent) or BioHPP pellets (bredent) (Brevest for2press, bredent).


\textsuperscript{22)} Ebd., 591.
\textsuperscript{23)} Ebd., 592.
\textsuperscript{24)} Ebd., 593.
\textsuperscript{25)} Ebd., 595.
\textsuperscript{26)} Ebd., 594.
\textsuperscript{27)} Ebd., 594.
\textsuperscript{28)} Ebd., 595.
After the breaking load measurement, the values were statistically evaluated using the single factor ANOVA and the Scheffé post-hoc test. In order to define and compare the reliability of the bridges, the Weibull statistics (Weibull module) were also calculated. In all tests, p-values of less than 5% were considered statistically significant. The data were analyzed with the statistical program SPSS, Version 20 (SPSS INC, Chicago, IL, USA).

Bridges machine-milled out of BioHPP blanks and bridges pressed from pellets showed higher mechanical stability than those pressed from BioHPP granules. Another advantage of CAD/CAM blanks is the industrial production of the material with a constant quality without porosity and inclusions. For BioHPP, the advantages of pressing technology are indication areas that are difficult to implement mechanically using CAD/CAM. Regardless of the manufacturing method, the three-unit PEEK/C bridges investigated delivered promising breaking load values for clinical application.

Editor’s note: “The high breaking load values can be achieved only with ceramic reinforced PEEK variants. The inorganic fillers are largely responsible for this. Comparable investigations of PEEK measured fracture loading values of 1.360 N. With the pressing technique, even more bond strength can be achieved by using mechanical retentions. Added to this is the greater flexibility in the fabrication of larger scaffold structures. The pressing technique also allows the fabrication of individual abutments using the overpressing process. Another advantage of the pressing technique is the production time, especially for larger scaffold constructions.”
5 Cleaning study of the scaffold material BioHPP\textsuperscript{29,30}  

This study examined the most suitable cleaning methods with regard to the tendency to discoloration. The commercial cleaning methods were divided into the areas of dentist, dental technology, and the possibilities of the patient in order to derive appropriate recommendations.

First, the test specimens (15 × 3 mm) were produced according to the manufacturer’s specifications. All test specimens were polished to a high gloss finish according to a material-specific polishing protocol. The quality of the polish was measured with a laser scanning microscope (Fig. 24). After the measurement all samples were stored in different suspensions (red wine, curry, chlorhexidine) at 37°C for 7 days. The samples aged in this way were measured with a colorimeter. This was followed by the cleaning of the samples using the various cleaning methods and the final measurement, indicating the roughness and degree of discoloration.

The surface of the scaffold material BioHPP can be polished significantly better than the surface of uni.lign and crea.lign. Furthermore, significantly fewer discolorations were detected with BioHPP than with uni.lign and crea.lign. The scaffold material can also be returned significantly better to its original colour by cleaning. The following methods have proven to be most suitable for cleaning BioHPP and uni.lign:

- **Patient:** soft and medium-hard toothbrush
- **Labside:** Needle cleaning and vibratory beaker
- **Chairside:** Air-Flow Comfort and Air-Flow Plus

\textsuperscript{31} Ebd.
\textsuperscript{32} Ebd.
\textsuperscript{33} Ebd.
\textsuperscript{34} Quick Reference Card für die Zahnarztpraxis. Leitfaden zur Orientierung bei der Anwendung von BioHPP. bredent GmbH & Co. KG, Senden; 2017.
BioHPP

![Graph showing discolouration rates of BioHPP according to the respective cleaning procedure.](image)

**Editor’s note:** “Patients with BioHPP dentures achieve the best cleaning performance when they use soft to medium-hard toothbrushes daily. This type of cleaning does not require roughening and subsequent polishing. The use of an ultrasonic tooth brush is not recommended because this leads to rougher surfaces. For the dental laboratory, the ultrasound baths and needle cleaning devices are best for cleaning dental prostheses made of BioHPP. Here, too, no subsequent polishing is necessary. In the dental practice, BioHPP surfaces can be cleaned with Air-Flow Comfort or Air-Flow Plus. The surfaces are somewhat roughened, which is why a subsequent high-gloss polishing should be carried out. Practical information on cleaning is given in the Quick Reference Card for the dental practice.”

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Fig. 26: Discolouration rates of BioHPP according to the respective cleaning procedure."
6 Formation of the oxide layer when pressing over pre-fabricated titanium abutments with BioHPP \(^{35}\)

In this paper the micro-structure change of pre-fabricated titanium components (Grade 4) used in the fabrication of individual single-tooth abutments using the overpress method was investigated. The processing protocol for overpressing requires an embedding with subsequent heat treatment. This heat treatment can negatively influence the mechanical properties of Grade 4 titanium.

In addition, the formation of an alpha-case layer and the formation of gaps between BioHPP and titanium abutment were investigated.

The titanium abutments (SKY elegance) were pressed over with the for2press system and BioHPP according to the manufacturer’s specifications. A maximum preheating temperature of 630°C was set for the 1st and 3rd series; a maximum of 850°C was set for the 2nd series. All specimens were embedded in plastic. Micrographs of these were prepared and examined under the microscope for structural changes. In addition, hardness progression measurements were carried out in order to be able to prove a possible hardening and thus structural change. The formation of titanium, aluminium and oxygen has been demonstrated using the EDX linear spectrum.

Two samples per modelation and series (10 samples in total) were examined. Neither the samples of the first nor the last series showed any significant alpha-case layer. There was only a thin layer of titanium oxide.

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\(^{36}\) Bilder bredent GmbH & Co. KG, Senden.


\(^{38}\) Ebd., 8.

\(^{39}\) Ebd., 11
In Series 2, an approx. 40-μm thick alpha-case layer was detected (Fig. 29). This can be seen from the low load hardness values determined (Fig. 30). Overall, the titanium structure underwent major changes. The grains of the alpha solid solution contained acicular oxygen-containing precipitates. These are produced by reaction with diffusing gases at higher temperatures. The relatively high proportion of Al2O3 particles (abrasive) on the abutment surface, which could influence the bond strength, must also be taken into account.

Editor's note: “The examination showed that at a preheating temperature of max. 630°C, no alpha-case layer is formed on the surface of the titanium abutment. An alpha-case layer is undesirable because its high hardness makes it brittle and can lead to cracks and late damage under stress. If the temperature of the pre-heating oven for the embedding mass ring is not controlled and a higher temperature is reached, intermetallic mixed crystals are formed inside the titanium structure. This structural change reduces the mechanical values and can damage the titanium abutment pressed over with BioHPP. The titanium alloy (Grade 4) of the SKY elegance abutment base meets these requirements and can be embedded, pre-heated, and pressed over.”
The aim of the study was to evaluate the behavior of non-veneered four-unit bridges made of fully anatomical PEEK. The two series to be investigated differed in the PEEK processing. In one series, the bridges were milled from PEEK; in the other series, they were pressed from PEEK. The main focus was on the dimensioning of the connector cross-sections in order to determine the maximum possible and sensible bridge span for definitively fixed BioHPP bridges.

In preparation for the examination, movable socketed plastic abutments with a gap width of 17 mm and a rounded step were manufactured (eight specimens per series). The abutments were then pretreated with Al2O3 at 110 µm/2 bar and H3eliobond (Ivoclar Vivadent). The inner sides of the bridge anchors were also prepared and additionally coated with visio.link (bredent). The bridges were then cemented using Variolink II (Ivoclar Vivadent). The three connector areas of the four-unit bridges (Fig. 31) were designed in the same way for all bridges examined.

The dimensions of the connector areas from palatal to buccal were 4.97 mm (1), 4.44 mm (2), and 4.95 mm (3) on average. The average diameter from occlusal to basal was 3.64 mm (1), 3.91 mm (2), and 3.73 mm (3). The average connector area was 13.55 mm² (1), 13.59 mm² (2), and 13.55 mm² (3). In the area of the pontics, the longest reinforcement section was located centrally in the area of the central fissure up to the basal support (Fig. 32). In previous tests, this design had proved to be optimal with regard to breaking strength.
After pre-treatment, the bonded bridges were subjected to artificial aging for a five-year clinical wearing period (1.2 × 10⁶ × 50 N mechanical loads and 2 × 3,000 × 5/55°C thermal alternating loads). The breaking load was measured with a tensile-compression testing machine (Zwick).

The breaking load at which the constructions failed was considered to be the values of the basal crack formation (see Fig. 33–35). Prior to the cracking of the bridges, acoustic failure indications occurred; these may indicate internal stresses of the system. The constructions yielded without visible damage. As a result of the bending of the bridges, veneering resins would have presumably flaked off at these load values.

The force required for basal crack formation was approx. 100 N higher (mean value) for milled bridges than for pressed bridges. It can be assumed that the milled constructions were less elastic (further force build-up after cracking up to the fracture possible) or had less internal stresses (no fracture noises).

With regard to the strength of the bridge constructions, a fully anatomical construction of tooth-coloured bridges made of PEEK is suitable as a possible metal-free restoration alternative.

Editor’s note: “Based on this study, the scaffold material BioHPP was approved for the indication of fixed bridges with a max. bridge span of 16 mm of unprepared abutment teeth. In addition, the connector surfaces should not fall below 14 mm² in the posterior region. To increase the bond strength between the veneering composite and the scaffold material, the longest reinforcement distance should lie between the central fissure and the basal support in order to be able to absorb the chewing forces well.”
In this study, the adhesive strength of different cementing materials (cements, adhesives, composites) depending on different cone angles (4°, 8°) and two different abutment materials (titanium, BioHPP) were investigated. Zirconia dioxide and BioHPP were used as crown materials. From the strength values determined, it was possible to determine whether a certain fastening material is suitable for temporary or definitive applications. The pretreatment of the abutments and crowns with various bonding agents was also analysed.

The titanium abutments were manufactured according to a sample from Straumann as the basis for the pull-off tests. The design resembled a pre-fabricated abutment with 4° or 8° cone angle. The samples were cleaned and eight copings with the different cements were fixed on each abutment. During cementing, the coping was subjected to a constant pressure of 15 N. The cemented samples were stored for 24 h in the incubator at 37°C under a moist cloth. They were then removed axially at 1 mm/min. In all cases, the samples were pre-treated in the dental laboratory using the equipment available there. The titanium abutments and BioHPP caps were blasted with 110 µm Al2O3. Eight test specimens with 4° and 8° were examined per group.

The following cements were tested:
1) Zinc oxide-eugenol-free (Temp-Bond, Kerr) without pre-treatment
2) Zinc oxide-eugenol-free (Temp-Bond, Kerr) with visio.link activation (polymerisation 90 s)
3) Silicone A based (TempoSIL 2, Coltène) without pre-treatment
4) Silicone A based (TempoSIL 2, Coltène) with visio.link activation (polymerization 90 s)
In the case of temporary fastening materials, TempoSIL 2 achieved a significantly higher (p < 0.007) adhesion force than Temp-Bond in all variants (Fig. 36). Only with TempoSIL 2 was there a significant difference (p = 0.025) between the angles of 4° and 8° when visio.link was used.

When Temp-Bond was used, the remaining cement content on the implant was always higher in the comparable groups with one exception (TempoSIL 2: 8°). If visio.link was used, the proportion of cement residue was always higher for Temp-Bond and always lower for TempoSIL 2 compared with the use without bonder.

Analogously, caps made from zirconia dioxide and BioHPP were bonded to definitive cements on BioHPP abutments of the same shape (Harvard zinc phosphate cement, Harvard; glass ionomer cement Ketac Cem, 3M).

During cementation, zirconia dioxide showed significantly (p<0.024) higher pull-off values in all groups compared with the cap materials. Only at 8° with Harvard mounting were there no significant (P = 1.000) differences between BioHPP caps and zirconia dioxide caps (Fig. 37).

After the pull-off test, cement residues of between approximately 10% (Ketac Cem/Zirkondioxid/4°+8°) and 55% (Ketac Cem/BioHPP/4°+8°) remained on the implant. When using the BioHPP coping, the residual cement values were generally higher than when using the zirconia dioxide coping. No difference could be found between the variants with 4° and 8°.

Editor's note: "TempoSIL 2 is very suitable for the temporary attachment of BioHPP to titanium abutments. With TempoSIL 2, the pre-treatment with visio.link is not necessary. For the definitive fixation of BioHPP to titanium abutments, a pre-treatment is recommended. The results of this study were also achieved when using Ketac Cem cement.

The results of this study were also achieved when using Ketac Cem cement.

Analogously, caps made from zirconia dioxide and BioHPP of the same shape (Harvard zinc phosphate cement, Harvard; glass ionomer cement Ketac Cem, 3M) were bonded to definitive cements on BioHPP abutments of the same shape.
The aim of the study was to assess the behaviour of four-unit bridges made of BioHPP with plastic veneers. The bridge scaffolds were made from granules from bredent using the for2press process. They differed in scaffold design, veneering material, and vertical abutment tooth height.

Several series of four-unit bridges were created and coupled to simulate physiological tooth mobility. The abutment bases were prepared with a circular step rounded on the inside. The residual stump height varied between 3 and 6 mm. After adhesive cementation of the bridges with Variolink II / Syntac Classic (Ivoclar Vivadent), the scaffolds were veneered with crea.lign (bredent). The samples were then subjected to chewing simulations and fracture tests.

In clinical use, even a basal crack formation was considered a form of failure because composite cracks can contribute to increased plaque retention and increased susceptibility to hydrolysis of the material as well as an increased risk of periodontitis and caries.

The bridge constructions with optimized veneers showed sufficient strength after chewing simulation and fracture tests. In the case of the optimized veneers, care was taken to ensure that they no longer protruded beyond the scaffold and had no sharp-edged ends and points at the connector areas.

Editor’s note: “When fabricating fixed bridges made of BioHPP and crea.lign veneers, particular attention should be paid to the morphological design. Breaking strength values between 600 and 1,100 Newtons can be achieved only by avoiding basal cracks. Based on these results and fracture patterns, a recommendation can be given with regard to processing.”

---

### Table: Fracture Patterns

<table>
<thead>
<tr>
<th>Bridge</th>
<th>F [N] Basal crack opening</th>
<th>F [N] max</th>
<th>Fracture pattern</th>
</tr>
</thead>
<tbody>
<tr>
<td>1</td>
<td>300</td>
<td>1092</td>
<td>Crack formation, no chipping, no scaffold fracture</td>
</tr>
<tr>
<td>2</td>
<td>600</td>
<td>2000</td>
<td>Total fracture of veneer/scaffold/abutment</td>
</tr>
<tr>
<td>3</td>
<td>800</td>
<td>2150</td>
<td>Veneering fracture</td>
</tr>
<tr>
<td>4</td>
<td>1000</td>
<td>1480</td>
<td>Veneering fracture</td>
</tr>
<tr>
<td>5</td>
<td>600</td>
<td>1950</td>
<td>Scaffold fracture</td>
</tr>
<tr>
<td>6</td>
<td>700</td>
<td>1830</td>
<td>Veneering fracture</td>
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<tr>
<td>7</td>
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<td>2660</td>
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</tr>
<tr>
<td>8</td>
<td>1100</td>
<td>1600</td>
<td>Veneering fracture</td>
</tr>
</tbody>
</table>

---

51) Ebd., 3.
52) Ebd., 6.
53) Ebd., 3.
56) Ebd., 3.
In vitro examination of three-unit standardised bridges

The chewing simulator was used to investigate the durability and breaking strength of standardised bridges after thermo-cyclic and mechanical loading. Various connector cross-sections were taken into account.

Identical molar stumps made of PMMA were fixed in pairs in plastic for periodontal support. To simulate a molar gap, the distance between the tooth stumps was approx. 10 mm. Using a plaster model, bredent produced identical standardised bridges from each bridge material. The bridges were fixed at the polyklinik after consultation with Variolink II (Ivoclar Vivadent). The bridges were subjected to a chewing simulation (1,200,000 × 50 N; 2 × 3,000 × 5°/55°C; H₂O, 2 min per cycle). A steatite sphere (d = 10 mm) was used as an antagonist. During the chewing simulation, the bridges were checked. Any failure was detected (with the corresponding number of chewing cycles), and the relative survival time was determined.

All the bridges examined survived the chewing simulation without visible damage. However, after simulation, the bridges showed clearly visible signs of wear in the contact area. Overall, the bridges examined showed fracture values that were significantly above the threshold value of 500N, which is usually required for posterior tooth applications. Ceramic restorations have similar or lower fracture values in comparison. In this context, it should be noted that maximum bending of the bridges at the fracture value can lead to clinical restrictions.

Editor’s note: “Because of the high breaking strength of BioHPP after chewing simulation (ageing), BioHPP can be used for fixed dentures. The connector cross-sections of 12 and 16mm² allow a delicate scaffold geometry with subsequent veneering. Aesthetics are not compromised in the interdental area. The breaking strength of BioHPP exceeds conventional ceramic scaffold materials by up to 1,000 Newtons”.

Fig. 41: Breaking force of the various test series.

Fig. 42: Tabular display of breaking force with mean value, standard deviation, minimum, and maximum.
In vitro examination of molar crowns on implants Influence of crown design with and without screw channel

In this in vitro study, the behaviour of molar crowns made of different materials in the chewing simulator (TCML) and their breaking strength after ageing was examined. The aim of the study was to test the influence of a screw channel on the stability and failure rate of the crowns and to test the suitability of the materials for use on implants in the posterior region.

Materials
Abutments: BioHPP elegance prefab (bredent);
crowns: a) HIPC (bredent): “HIPC”; b) crea.lign on anatomically reduced BioHPP scaffold (bredent): “CREA”; c) IPS e.max (Ivoclar Vivadent): “EMAX”

The implants (SKY implant analogue, bredent medical) were fixed vertically in specimen holders, whereby the construction of the natural jawbone from compact bone and cancellous bone was simulated by the plastics PEEK and POM. Fully anatomical crowns for the posterior region were fabricated from the materials mentioned above (n = 8 for TCML, n = 2 for 24 h).

Eight crowns were each provided with a screw channel (diamond drill, d = 2 mm) and then adhesively cemented onto identical, pre-treated BioHPP abutments. The screw channel of the respective crowns was closed with composite (Filtek Supreme, 3M).

All samples were then subjected to a thermal alternating load (5°/55°C, 2 min/cycle) as well as a mechanical alternating load in the chewing simulator (TCML; 50 N; 1.6 Hz). Steatite spheres (d = 12 mm) served as standardised antagonists.

All samples of the HIPC and EMAX series survived the simulation without failures. In group CREA, 960,000 chewing cycles (i.e. an estimated wearing time of 4 years) resulted in a fracture of the crown (Fig. 44).

Fig. 43: Milled abutment made of a BioHPP elegance prefab.

Fig. 44: Crown failure during chewing simulation after 960,000 cycles.
The failure patterns were connected by a fracture or by a fracture combined with a complete loosening of the crown.

The HIPC and EMAX crowns survived the 5-year in vitro simulation without failures. Of the crown variants examined, the HIPC variants showed the highest breaking strength values (Fig. 46). The screw channel significantly weakened the design of both variants investigated.

Editor’s note: “Especially for immediate implant placement and immediate restoration, a shock-absorbing BioHPP elegance hybrid abutment is ideal for restorations with aesthetic and hard e.max crowns”.

<table>
<thead>
<tr>
<th></th>
<th>Screwed</th>
<th>Bonded</th>
</tr>
</thead>
<tbody>
<tr>
<td>HIPC</td>
<td>8 x crown fracture</td>
<td>6 x completely detached</td>
</tr>
<tr>
<td></td>
<td></td>
<td>2 x crown fracture</td>
</tr>
<tr>
<td>CREA</td>
<td>1 Failure: Crown fracture</td>
<td>-</td>
</tr>
<tr>
<td></td>
<td>7 x crown fracture</td>
<td></td>
</tr>
<tr>
<td>EMAX</td>
<td>6 x completely detached</td>
<td>2 x completely detached</td>
</tr>
<tr>
<td></td>
<td>2 x crown fracture</td>
<td>6 x crown fracture</td>
</tr>
</tbody>
</table>

Fig. 45: HIPC, CREA, and EMAX series failure patterns.⁶⁴

Fig. 46: An overview of the fracture values.⁶⁵
12 Bacterial attachment to BioHPP

Prof. Dr. J. Geis-Gerstorfer, Dr. L. Scheideler
Eberhard Karls University, Tübingen
Centre for Oral and Maxillofacial Medicine, Department of "Medical Materials Science & Technology"

In the project, the plaque build-up on the PEEK material BioHPP was to be investigated in comparison to other scaffold and veneering materials.

For this purpose, test specimens were exposed to oral bacteria cultures, and the bacterial deposition was optically documented and quantified. In the study, the samples were incubated with different micro-organisms in constant alternation of movement and stagnation. The conditions in the niches of the oral cavity (e.g. interdental spaces) were to be simulated. The experiments were performed with Streptococcus gordonii (as a typical early colonizer of the oral cavity) as well as fresh isolates of mixed oral cultures. Three different dental PMMA-based plastic materials (top.lign, novo.lign, crea.lign) as well as zirconia oxide were used as reference materials. The zirconia oxide was also tested in two different states (ZrO2 colored and ZrO2 CAD/CAM).

The aim of the investigation was to produce surface states that are similar to the real machining state of dental restorations in practice. Accordingly, surface treatment and cleaning were carried out at bredent according to current dental technology methods.

The experiments carried out with different test kits or dyes for bacterial quantification via substrate turnover (metabolic activity) showed some promising approaches but proved to be too insensitive and poorly reproducible in the test system used here. These approaches therefore had to be abandoned after some preliminary tests. The crystal violet staining proved to be the most reproducible detection method despite the problems caused by the surface conditions of the samples in this project.

Adhesion Streptococcus Gordonii (summary)

![Graph showing bacterial attachment to different materials](image)

Fig. 47: Initial colonisation by S. gordonii. Summary of data from two trials. Adhesion time: 2 h. (mean values with standard deviations; n = 6; star = significantly different from BioHPP CAD/CAM; p = 0.05).
S. gordonii showed a significantly lower deposition on the surfaces of BioHPP (pressed) and novo.lign compared to the reference surface BioHPP CAD/CAM (Fig. 47). The strongest accumulation on average was measured on the reference plastic crea.lign. Compared with BioHPP CAD/CAM, the detectable amount of adhered bacteria was approximately double that of BioHPP CAD/CAM (184%).

The bacteria were stained with crystal violet. Fig. 48 shows the extent of biofilm formation on the various surfaces by S. gordonii. A typical platelet was documented for each surface. On the left side, an overview image is shown; on the right side, a detailed image is shown. It is clearly visible that in the experiments with S. gordonii, the pressed BioHPP surface has a significantly lower occupancy than the CAD/CAM surface. The relatively strong, continuous bacterial coating on crea.lign is also clearly visible in comparison to the novo.lign surface shown above. S. gordonii also showed a relatively pronounced adhesion on the investigated zirconia oxide surfaces.

The results of the CCK-8 assay correlated well with the subsequent crystal violet staining on the same samples. The substrate turnover data (Fig. 49) showed the same trends as the summarized results of bacterial staining by crystal violet (Fig. 47). S. gordonii deposited less on BioHPP (pressed) and novo.lign significantly less than on the reference surface BioHPP CAD/CAM. The strongest accumulation on average was again measured on crea.lign.

Editor’s note: “From these results, it can be concluded that exposed BioHPP scaffold geometries in the oral cavity are no more populated with plaque and bacteria than those made of zirconia or veneering composites. This requires a high-gloss polished surface. For rough surfaces, the results may be different.”

**Streptococcus Gordonii Adhesion (metabolic activity CCK-8)**

![Graph showing metabolic activity CCK-8](image)

Fig. 49: Initial colonisation by S. gordonii. Metabolic activity test. Adhesion time: 2 h. (mean values with standard deviations; n = 3).

Abb. 48: Vergrößerte Darstellung der Ergebnisse einer Versuchsreihe zur Bakterienbedeckung mit S. gordonii.
In this in vivo clinical study, 35 patients with a total of 213 implants were immediately treated with a temporary PMMA bridge according to the SKY fast & fixed concept. After 15 to 16 weeks, the final restoration was either a rigid metal composite bridge (Fig. 51 left) or a physiological ceramic-reinforced PEEK composite bridge (Fig. 51 right).

The objective of the study was to determine the degree of bone loss. The peri-implant bone level was measured at three points in time (see Fig. 50): directly after implant placement, after 3–4 months for the final prosthetic restoration, and after 1 year for the recall. The measurement was carried out according to a standardised procedure.
Treatment with implants guarantees long-term functionality and aesthetics. Sufficient strength of stable bone substance and a suitable gum environment are basic prerequisites for long-term success.

The results of the investigation show that a considerably low bone loss can be observed on the x-ray images when using PEEK. Fig. 52 shows the differences in bone loss in prostheses with metal and PEEK scaffolds.

Editor’s note: “The PEEK material tested is BioHPP, a ceramic-reinforced PEEK variant. Because BioHPP is characterised by bone-like elasticity, the force absorption is comparable to that of natural bone. BioHPP can therefore absorb the chewing forces and other loads and does not transfer them directly to the implant.”

Fig. 52: Bone loss with PEEK prostheses is less than with metal prostheses.
Uses of PEEK in dentistry are still under development; the material has been mainly employed for implant abutments. The aim of this study was to examine the application of polymer-based abutments for definitive dental restorations through a single protocol connection, using two surgical techniques (standard and flapless).

Traditionally, abutments have been made from biocompatible materials such as titanium and other metal alloys. Other therapeutic options include customized abutments based on ceramics or zirconia. But neither of these is suitable for the one-stage approach in which the implant is immediately restored after placement.

In this study ten blueSKY implants (bredent medical, Senden, Germany) with 3.5 to 4 mm of diameter and 10 to 12 mm of length were randomly crestally placed in the premolar zone (P1 or P2) of the maxillary bone. Furthermore ten BioHPP SKY elegance abutments were connected at the time of implant placement (immediate loading). BioHPP SKY elegance abutments are hybrid abutments in which the abutment body made of BioHPP is connected to the titanium base without gap. These abutments are used in single-stage treatment (immediate restoration), since they combine the properties of a temporary and a definitive abutment, i.e. it is not necessary to change the abutment. All crowns were produced from feldspatic ceramic (IPS Empress CAD Cerec/InLab) using a Cerec system and cemented using self-adhesive Rely-X universal cement.

Radiological analysis
Standardized radiographs were taken on the day of implant placement and at one, three and five months using a paralleling system. The radiological analysis was performed with the ImageJ software (Wayne Rasband, USA). The distances between the platform and the first bone contact were recorded (Fig. 55).

Fig. 55 show previous CT scans (left) of the sample case and radiological analysis after implant placement (right). No bone loss surrounding the implants is observed. A good stability of bone height can be appreciated. Fig. 56 lists length measurements between the implant platforms and the points of first bone contact.

ISQ analysis
Stability measurements were made at baseline to assess the stability of the implant to examine whether immediate loading was feasible. An ISQ value of 65 was defined as a minimum. The ISQ values were obtained using Osstell Mentor (Osstell, Göteborg, Sweden).
Fig. 56: Radiological analysis of samples. The results are presented as mean ± SD (median). A non-parametric Friedman test.

Fig. 57 lists the ISQ values for the implants on the day of placement. All implants showed values above the minimum established for this study (ISQ of 65).

Mucogingival analysis and clinical findings
The bleeding index for the implants was recorded at one, three and five months after implant placement by means of a special peri-implant probing technique. Moreover, any post-insertion loss of periimplant mucosa and any height loss were recorded. Bleeding on probing (0 = none, 1 = present) was also tested for at one, three and five months. Insertion lengths were measured using a conventional plastic probe, with the same investigator taking six measurements for each implant. The results are presented as the means of six measurements.

Fig. 58 lists gingival and bleeding indices for all implants. No implant exhibited retractions or insertion loss. The insertion length is listed in Table 4. Greater length was observed in the standard group compared with the flapless group and no significant differences were observed between different times within each group.

No abnormal clinical signs of inflammation were observed at the time of review of the study. There was complete adaptation of the peri-implant soft tissue to the crown and the emergence profile of the BioHPP SKY elegance abutment. With the flapless protocol (Figs. 2a to h), the healing process was faster than with the standard protocol (Figs. 3a to c), but towards the end it was similar.
The BioHPP SKY elegance abutment interacts perfectly with the peri-implant tissue, as evidenced by the absence of swelling and faster healing of the soft tissue. This biocompatibility is one of the most evident and appreciated data obtained from this study and from a review of the literature.

Editor’s note: “Within the limitations of a clinical pilot study in terms of sample size, it can be concluded that the BioHPP SKY elegance abutment is an ideal solution for those implant cases where immediate loading with a definitive restoration in a single session is performed; it provides high levels of biocompatibility, mechanical and flexural strength and elasticity and achieves highly aesthetic results.”
15 In-vivo study: Peri-implant tissues behavior around non-titanium material: Experimental study in dogs\textsuperscript{78}

José Eduardo Maté
Sánchez de Val
Carlos Pérez Albacete
Martínez Sergio Gehrke
María P. Ramírez Fernández
Vicente G. Vicent
Gerardo Gómez Moreno
José L. Calvo Guirado
Universidad Católica San Antonio
de Murcia (UCAM)
Biotecnos-UCAM Research Center
University of Granada

Six male American Foxhound of approximately one year of age, each weighing approximately 14–15 kg, were used for this study. Forty-eight tapered dental implants (blueSKY, bredent medical, Senden, Germany) with internal connection and 3.5 mm in diameter and 10 mm length with a collar of 0.7 mm length. All implants were fitted with abutments immediately after placement and divided into two groups. Control group that received 24 titanium abutments and a test group that received 24 PEEK reinforced abutment (SKY elegance, bredent medical, Senden, Germany).

Eight weeks after surgery, all implants showed suitable primary stability. No statistically relevant differences were found between the groups; all implants were osseointegrated. The gaps between the implant and alveolus created by the insertion were filled with bone and absorbed by the alveolar ridge.

In both groups, the formation in the marginal defect zone was accompanied by significant dimensional loss of the bone – both in the delicate buccal region and in the more substantial lingual region.

The test group (reinforced PEEK abutment) showed the best results in soft tissue stabilisation in both lingual and buccal analysis. The radiological examination confirmed the results of the histological analysis at the bone level: In the two groups (titanium and PEEK), a greater loss of buccal bone was observed compared with the lingual bone.


Fig. 60: On the left, the soft tissue is attached to a titanium abutment; on the right, it is attached to a BioHPP abutment. On the right, the higher level of soft tissue is clearly visible lingually.\textsuperscript{79}

\begin{align*}
PM &= \text{Peri-implant mucosa} \\
IS &= \text{Implant shoulder} \\
LC &= \text{Lingual bone crest} \\
BC &= \text{buccal bone crest}
\end{align*}
### SUMMARY OF SCIENTIFICAL RESULTS

<table>
<thead>
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<th>Titanium</th>
<th>PEEK</th>
<th>p-value</th>
</tr>
</thead>
<tbody>
<tr>
<td>PM-Bc</td>
<td>2.74 ± 0.41</td>
<td>3.11 ± 0.26*</td>
<td>0.032</td>
</tr>
<tr>
<td>PM-Lc</td>
<td>2.74</td>
<td>3.11</td>
<td></td>
</tr>
<tr>
<td>PM bucal-IS</td>
<td>2.91 ± 0.03</td>
<td>3.71 ± 0.18*</td>
<td>0.008</td>
</tr>
<tr>
<td>PM lingual-IS</td>
<td>2.91</td>
<td>3.71</td>
<td></td>
</tr>
<tr>
<td>IS-Bc</td>
<td>2.35 ± 0.87</td>
<td>2.95 ± 0.53*</td>
<td>0.015</td>
</tr>
<tr>
<td>IS-Lc</td>
<td>2.35</td>
<td>2.95</td>
<td></td>
</tr>
<tr>
<td>PM bucal-IS</td>
<td>2.65 ± 0.43</td>
<td>3.57 ± 0.38*</td>
<td>0.003</td>
</tr>
<tr>
<td>IS-Lc</td>
<td>2.65</td>
<td>3.57</td>
<td></td>
</tr>
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<td>IS-BC</td>
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<td>1.53 ± 0.21</td>
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</tr>
<tr>
<td>IS-LC</td>
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<td>1.53</td>
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<td>ISQ Value Insertion</td>
<td>Mean ± Sd</td>
<td>Median</td>
<td>Mean ± Sd</td>
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<tr>
<td>BioHPP abutment</td>
<td>74.46 ± 4.55</td>
<td>74.46 ± 4.55</td>
<td>69.53 ± 0.47</td>
</tr>
<tr>
<td>Titanium abutment</td>
<td>74.19 ± 4.29</td>
<td>74.19 ± 4.29</td>
<td>70.80 ± 0.67</td>
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<tr>
<td>BIC (%) Titanium PEEK</td>
<td>Mean ± Sd</td>
<td>PEEK</td>
<td>p-value</td>
</tr>
<tr>
<td>Mean ± Sd</td>
<td>61.29 ± 1.45</td>
<td>62.52 ± 4.63</td>
<td>0.32</td>
</tr>
<tr>
<td>Median</td>
<td>61.29</td>
<td>62.52</td>
<td></td>
</tr>
</tbody>
</table>

Fig. 61: Linear measurements in millimeter.\[80]\n
\[80]\) Sanchez, Periimplant tissues behavior, EAO Congress 2016.

Fig. 62: Friedman test of BSQ analysis and measurements at initial day and at 8 weeks. Results as mean and medians. (\*) Significant differences, p<0.05.\[81]\n
Fig. 63: Friedman test of BIC values comparison between Titanium and Hybrid PEEK-Ti abutments implant placement at 8 weeks follow-up period. Data shows mean, SD and medians. (\*) Significant differences, p<0.05. No differences were found.\[82]\n
\[81]\) Ebd.

\[82]\) Ebd.
The application of reinforced titanium peek abutments gives a great aesthetic advantage over other conventional materials; the white color of the abutment allows handling situations involved in fine gingival biotypes without the restrictions of conventional titanium abutments. The materials of high biocompatibility rate, can be used immediately to surgery: “one abutment one time”. Quantitative histomorphometric assessment of soft tissue analysis showed that there are differences in favor of peek abutments, with greater height and peri-implant soft tissue thickness, which is important because it implies that there was not peri-implant bone loss and the establishment of biological seal is achieved for the abutment.

*Editor’s note: “With the limitations of animal experimentation, it can be concluded that the PEEK reinforced with titanium abutments constitute an effective alternative to conventional abutments, given its high rate of biocompatibility and can preserves bone height and soft tissue stability.”*

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**Table 1:** Radiological analysis of bone first contact distance to the implant shoulder. Values as Mean ± Sd and Median. Non parametric Friedman test analysis. Significant differences with $p<0.05$.

<table>
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<th>Titanium</th>
<th>PEEK</th>
<th>$p$-value</th>
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<tr>
<td><strong>Bucal bone</strong></td>
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<td></td>
<td></td>
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<tr>
<td>Mean ± Sd</td>
<td>1.96 ± 0.21</td>
<td>1.43 ± 0.11</td>
<td>0.013</td>
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<tr>
<td>Median</td>
<td>1.96</td>
<td>1.43</td>
<td></td>
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<tr>
<td><strong>Lingual bone</strong></td>
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<td></td>
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<tr>
<td>Mean ± Sd</td>
<td>1.78 ± 0.33</td>
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<td>0.031</td>
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<tr>
<td>Median</td>
<td>1.78</td>
<td>1.28</td>
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